

# Spectral Graph Wavelets on the Cortical Connectome and Regularization of the EEG Inverse Problem

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# Overview

## Spectral Graph Wavelet Transform (SGWT)

Motivations from Classical Wavelet Analysis

Spectral Graph Theory

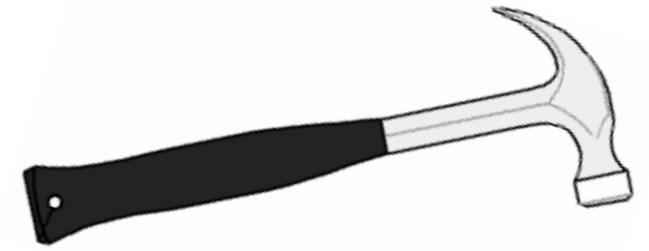
SGWT construction

## EEG source estimation

Electrical head modeling

Cortical connectome graph construction

Sparse representation with Cortical Spectral Graph Wavelets



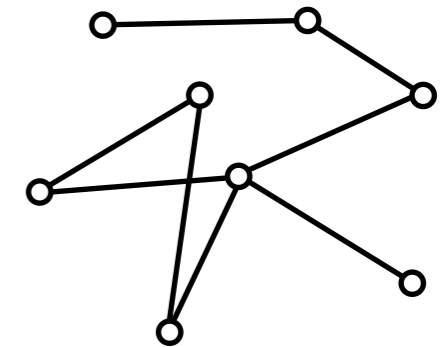
# SGWT : wavelets on weighted graphs

Weighted graphs :

$N$  vertices

Symmetric adjacency matrix

$$A_{i,j} = w_{i,j} \quad (w_{i,j} \geq 0)$$



$f(i)$  : value on  $i^{th}$  vertex

Wavelets on weighted graph:

Linear, multiscale representation for functions on vertices  $f \in \mathbb{R}^N$

$\psi_\gamma \in \mathbb{R}^N$  localized in space and frequency

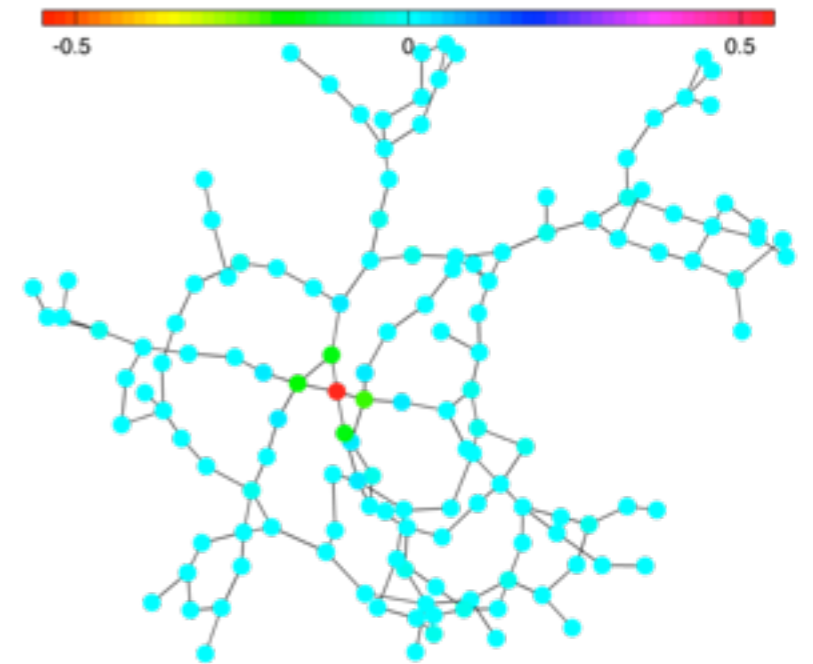
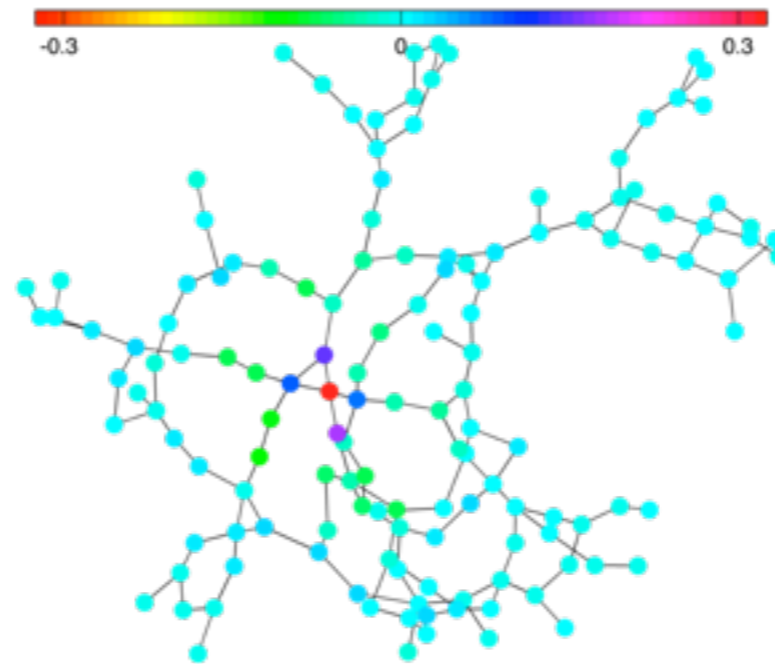
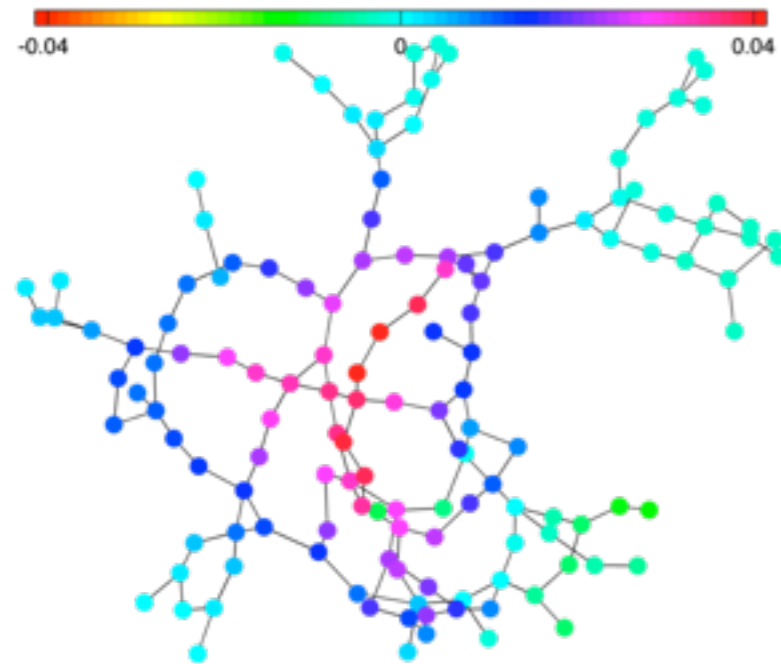
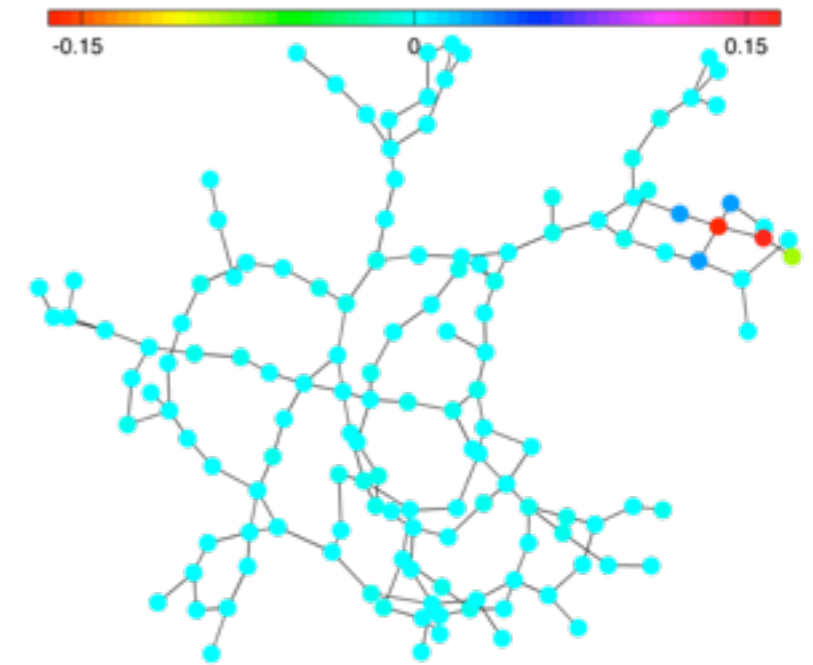
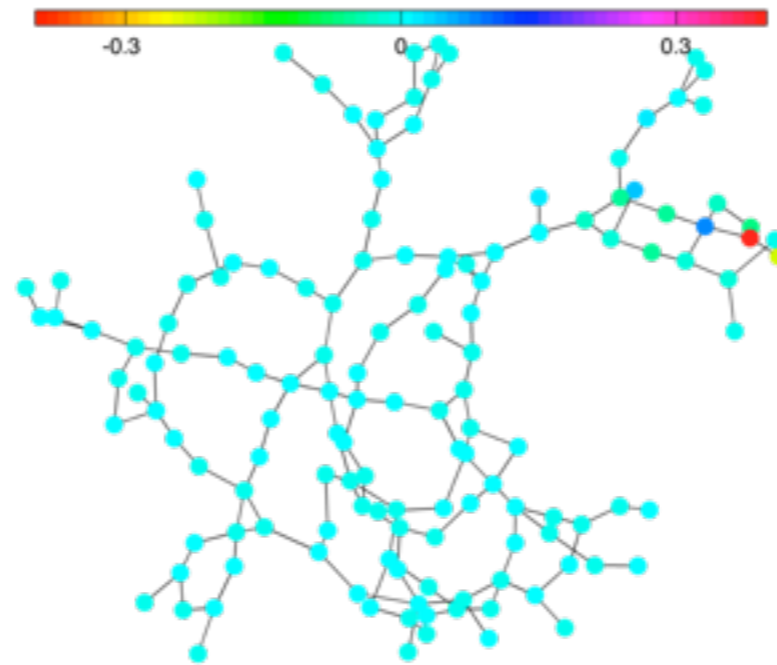
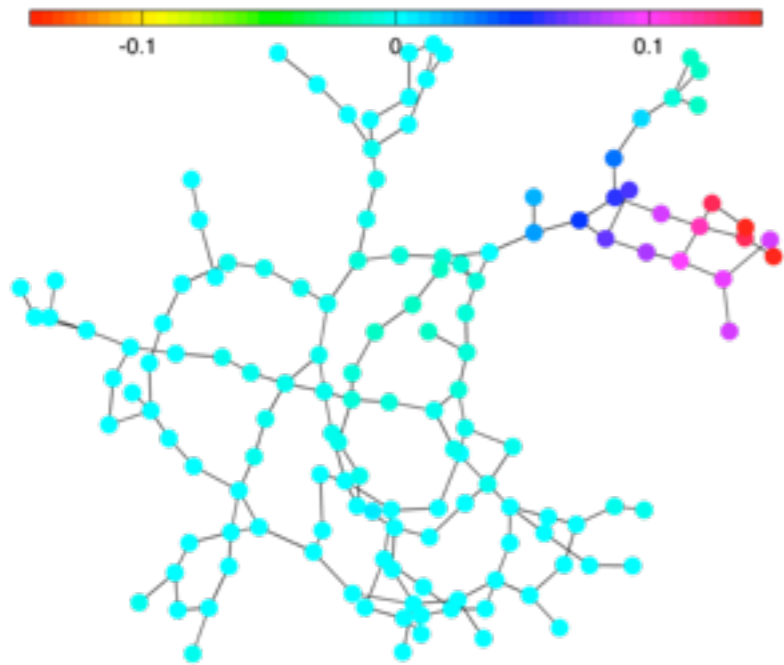
$$c_\gamma = \langle \psi_\gamma, f \rangle$$

Why?

Wavelets : very useful, but classically limited to Euclidean space

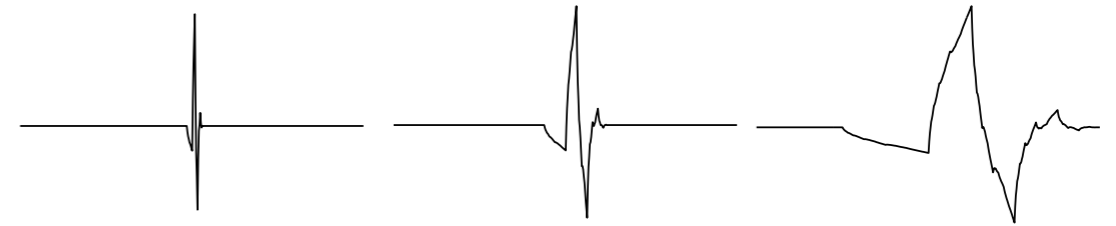
Graphs : flexibly model complicated data domains

# Preview : some SGWT graph wavelets



# Classical wavelet analysis

Signal  $f \in L^2(\mathbb{R})$



translation & dilation

$$\psi_{t,u}(x) = \frac{1}{\sqrt{t}} \psi \left( \frac{x - u}{t} \right)$$

Analysis : wavelet coefficients

$$W_f(t, u) = \langle \psi_{t,u}, f \rangle$$

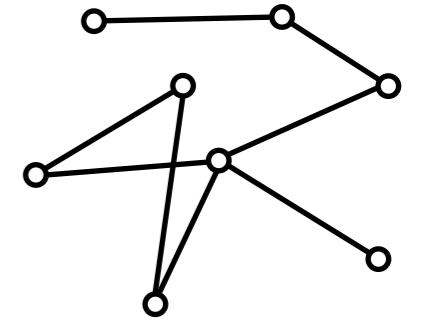
Reconstruction (Orthogonal Wavelet case)

$$f = \sum_{n,j} W_f(2^j, 2^j n) \psi_{2^j, 2^j n}(x)$$

Signal manipulation often easier in wavelet transform space

# Towards Wavelets on Graphs

Problem : dilation and translation on irregular Graph?



Wavelet transform in Fourier domain :

$$W_f(t, x) = f \star \bar{\psi}_t$$

$$\bar{\psi}_t(x) = \frac{1}{t} \psi\left(-\frac{x}{t}\right)$$

$$\widehat{W_f(t, \omega)} = \hat{f}(\omega) \underline{\hat{\psi}^*(t\omega)}$$

Individual wavelets : apply operator to  $\delta_u(x) = \delta(x - u)$

$$\begin{aligned} \psi_{t,u}(-x) &= W_{\delta_u}(t, x) \\ &= \mathcal{F}^{-1} \left( \underbrace{\hat{\delta}_u(\omega)}_{\text{localization}} \underbrace{\hat{\psi}^*(t\omega)}_{\text{dilation}} \right) \end{aligned}$$

**Dilate operator  $\hat{\psi}^*(t\omega)$  in frequency domain, then localize**

Analog of Fourier transform on weighted graphs => Spectral graph theory

# Spectral Graph Theory

Degree matrix

$$D_{i,i} = \sum_{k=1}^N A_{k,i}$$

Graph Laplacian

$$L = D - A$$

Spectral decomposition of  $L$

$$L\chi_l = \lambda_l\chi_l \quad 0 = \lambda_1 \leq \lambda_2 \leq \dots \leq \lambda_N$$

$$\{\chi_l\}_{l=1}^N \quad \text{orthonormal basis}$$

Graph “Fourier transform”

$$\hat{f}(l) = \langle \chi_l, f \rangle = \sum_n \chi_l^*(n) f(n)$$

Graph “inverse Fourier transform”

$$f = \sum_l \hat{f}(l)\chi_l$$

# Spectral Graph Wavelets

Wavelet kernel  $g : \mathbb{R}^+ \rightarrow \mathbb{R}^+$

analogous to  $\hat{\psi}^*(\omega)$

Wavelet operator (at scale  $t_j$ )

$$T_g^{t_j} = g(t_j L) : \mathbb{R}^N \rightarrow \mathbb{R}^N$$

Action defined on eigenvectors

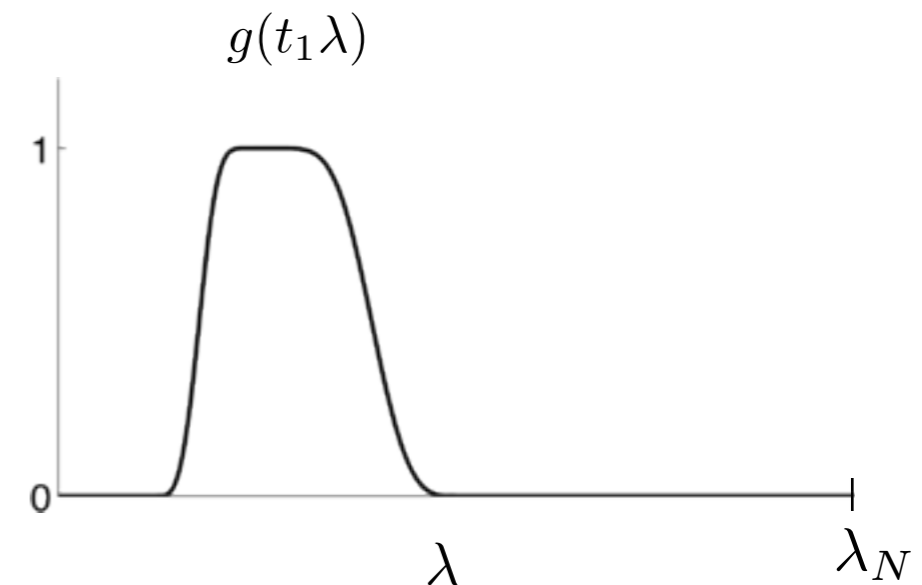
$$T_g^{t_j} \chi_l = g(t_j \lambda_l) \chi_l$$

Wavelets

$$\psi_{j,n} = T_g^{t_j} \delta_n$$

SGWT coefficients at scale  $j$

$$T_g^{t_j} f = \sum_l g(t_j \lambda_l) \hat{f}(l) \chi_l$$



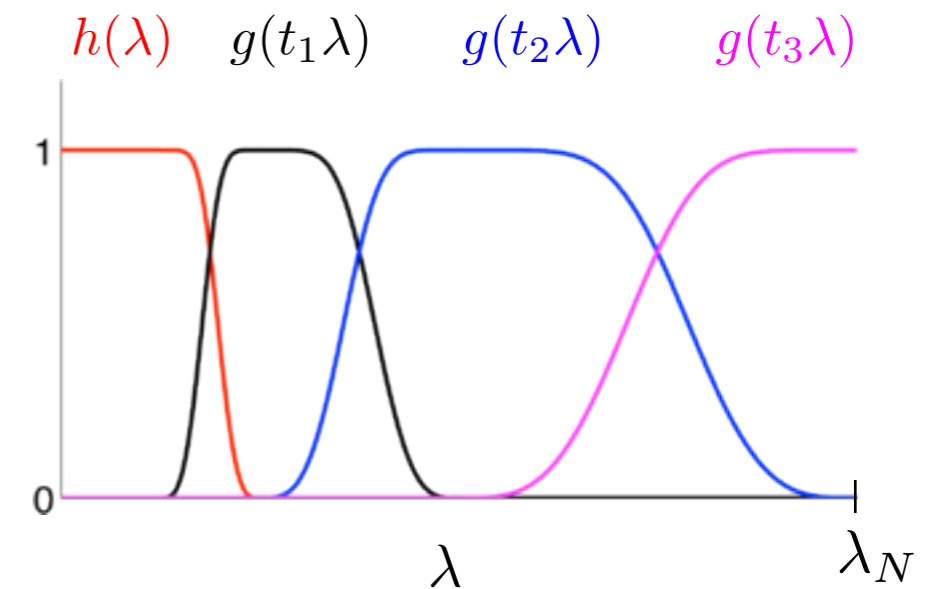


# Spectral Graph Wavelets

Scaling function band

$$T_h = h(L)$$

$$\phi_n = T_h \delta_n$$



K-fold Overcomplete

$$W : \mathbb{R}^N \rightarrow \mathbb{R}^{KN}$$

**K=4**

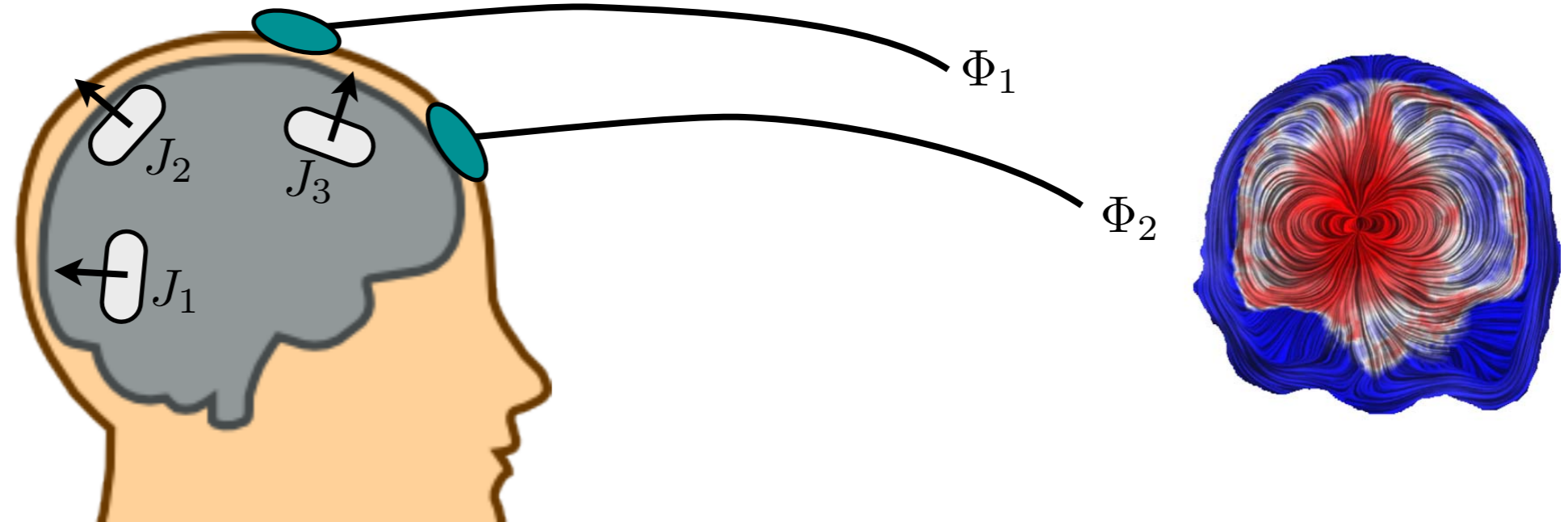
Fast SGWT

Polynomial approximation of  $g(t_j x)$

Avoids diagonalization of  $L$

# Application to EEG Source Estimation

# Electroencephalography (EEG)



EEG signal : arises from dipole current sources + volume conduction

Source estimation : Infer current sources  $J$  from electrode measurements  $\Phi$

Access to subject specific brain anatomy :

MRI : measure tissue geometry

Diffusion tensor imaging (DTI) + tract tracing : measure brain connectivity

How to exploit connectivity knowledge? Sparsity in cortical graph wavelet basis.

# EEG forward problem

Quasi-static Maxwell PDE

$$\nabla \cdot (\sigma \nabla \phi) = s$$

$\phi$  : potential

$s$  : current sources

$\sigma(x, y, z)$  : tissue conductivity

$$(\sigma \nabla \phi) \cdot \vec{n} = 0 \quad \text{on boundary}$$

Finite-difference solver, on 1mm 3D grid

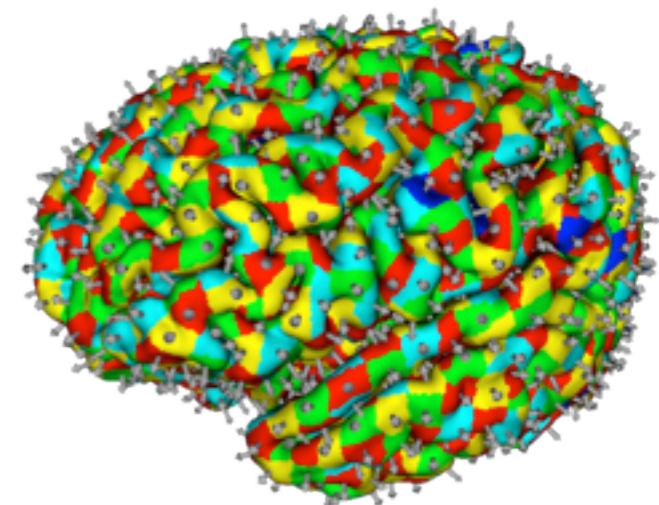
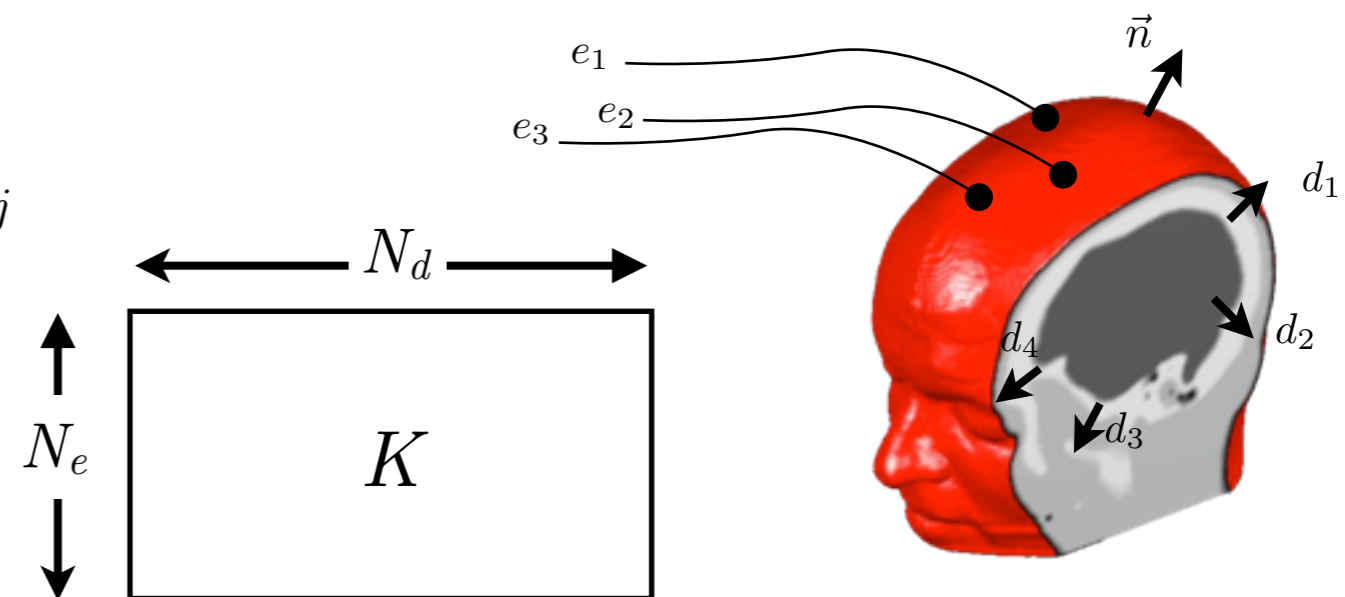
Lead field matrix  $K$

$K_{ij}$  : solution at  $e_i$  with unit source at  $d_j$

$$\Phi = KJ$$

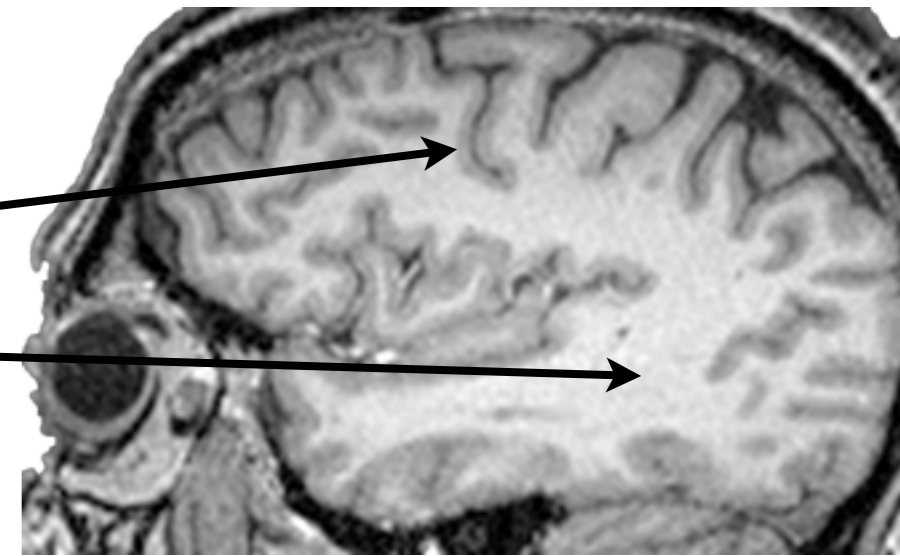
$J \in \mathbb{R}^{N_d}$  : source current amplitudes

$\Phi \in \mathbb{R}^{N_e}$  : electrode voltages

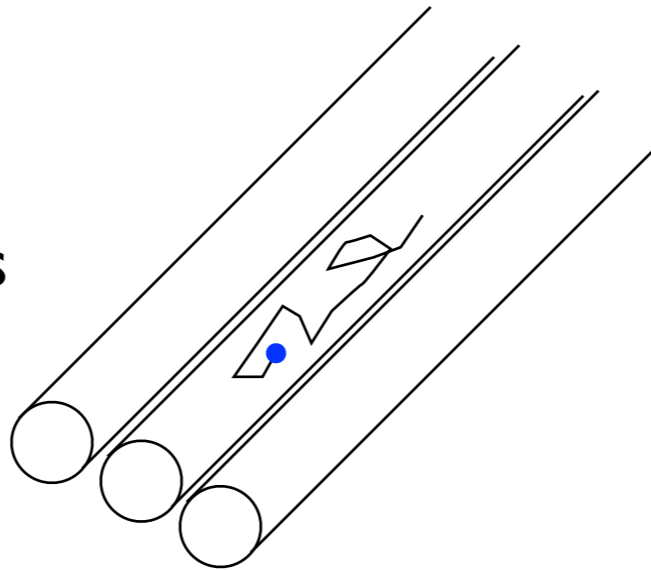


# Cortical connectome graph

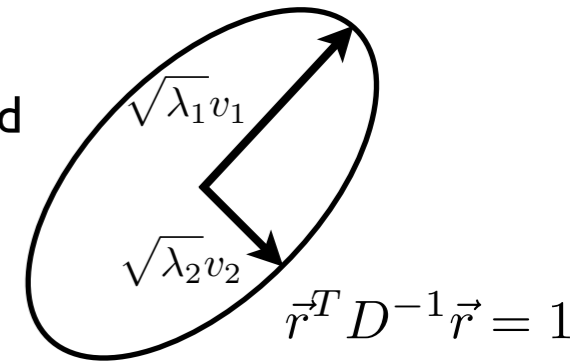
Cortical grey matter (neuron cell bodies)  
connected by white matter fibers (axons)



Diffusion along fiber directions



diffusion ellipsoid



Diffusion Tensor Imaging (DTI) measures water diffusion direction at every voxel

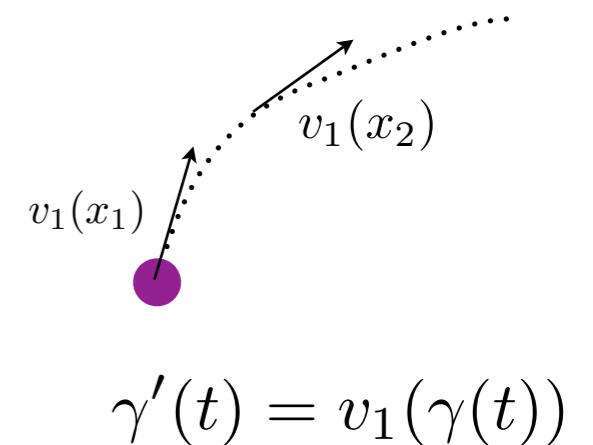
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## Tractography

dominant eigenvector  $v_1$  reveals fiber orientation

compute streamlines, from seed points

( a little more complicated, in practice ... )





# Cortical connectome graph

seed in white matter, retain tracts connecting cortex to cortex

global (tract-based) connectome  $A^{tr}$

$$a_{i,j}^{tr} = \sum_{k \text{ connecting } i \text{ and } j} \frac{1}{\text{length}(k)}$$

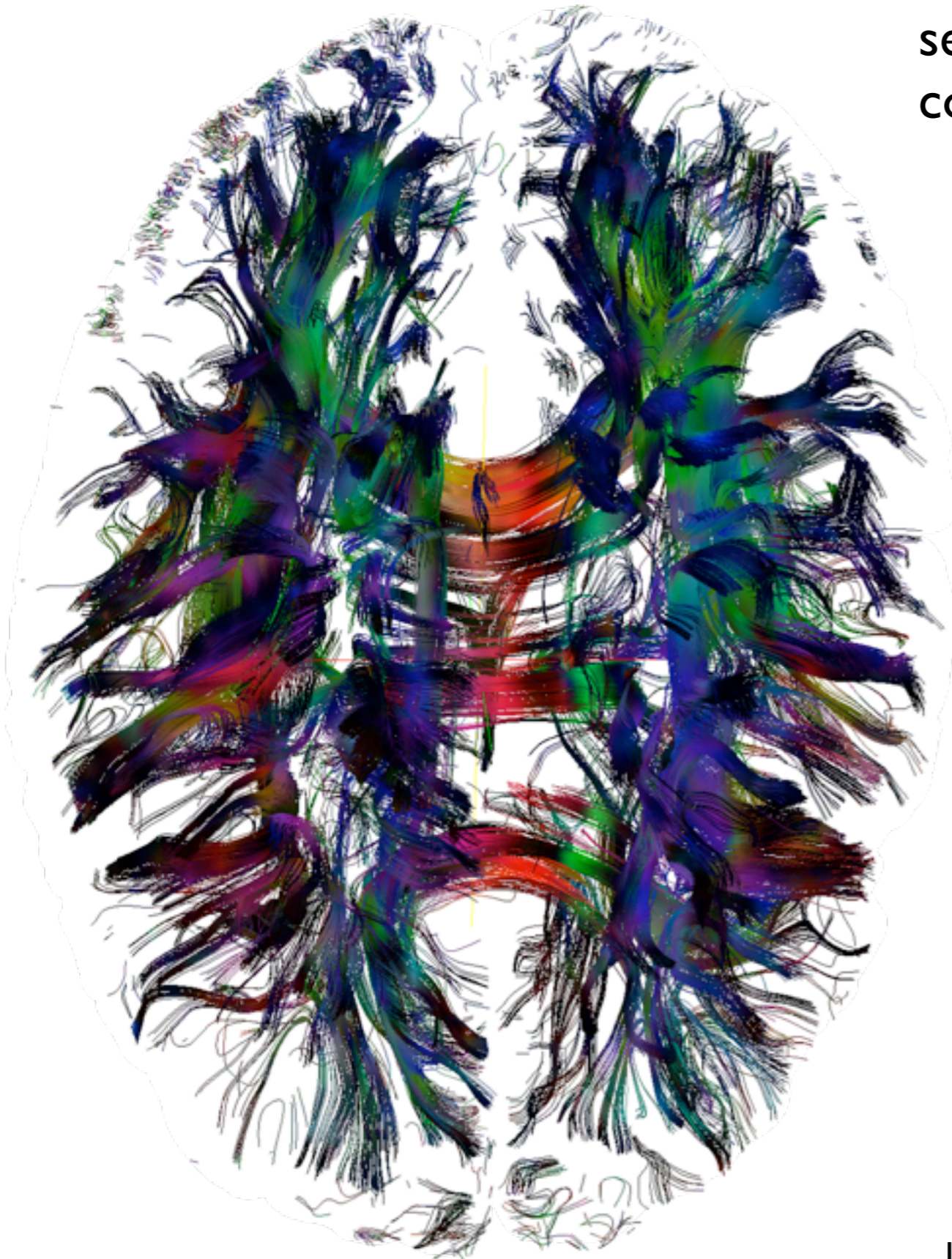
local (adjacency-based) connectome  $A^{loc}$

$$a_{i,j}^{loc} = \text{length of boundary between patches } i,j$$

hybrid connectome  $A$

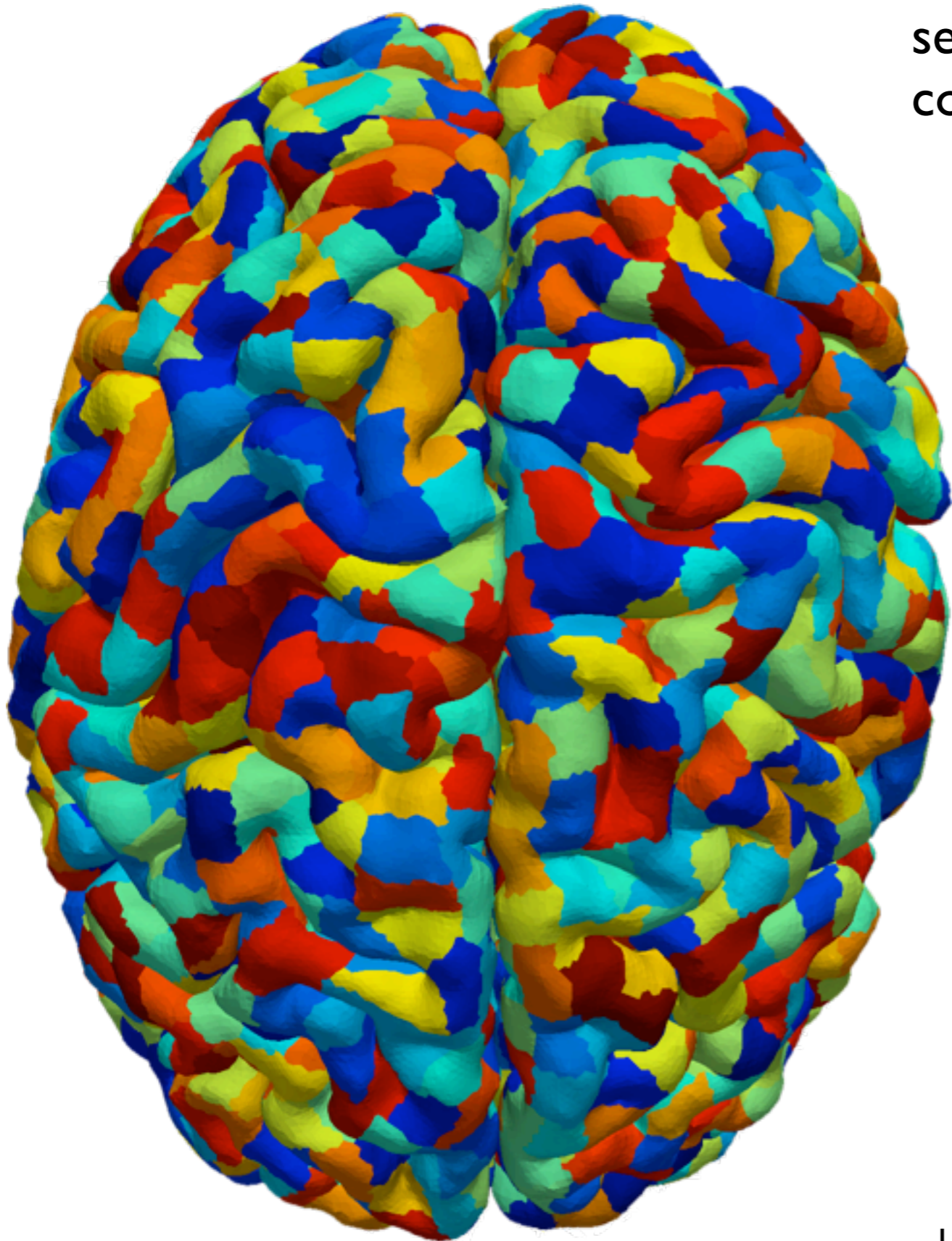
$$A = \lambda_{tr} A^{tr} + \lambda_{loc} A^{loc}$$

showing 12,124 out of 775,939 cortical-cortical tracts





# Cortical connectome graph



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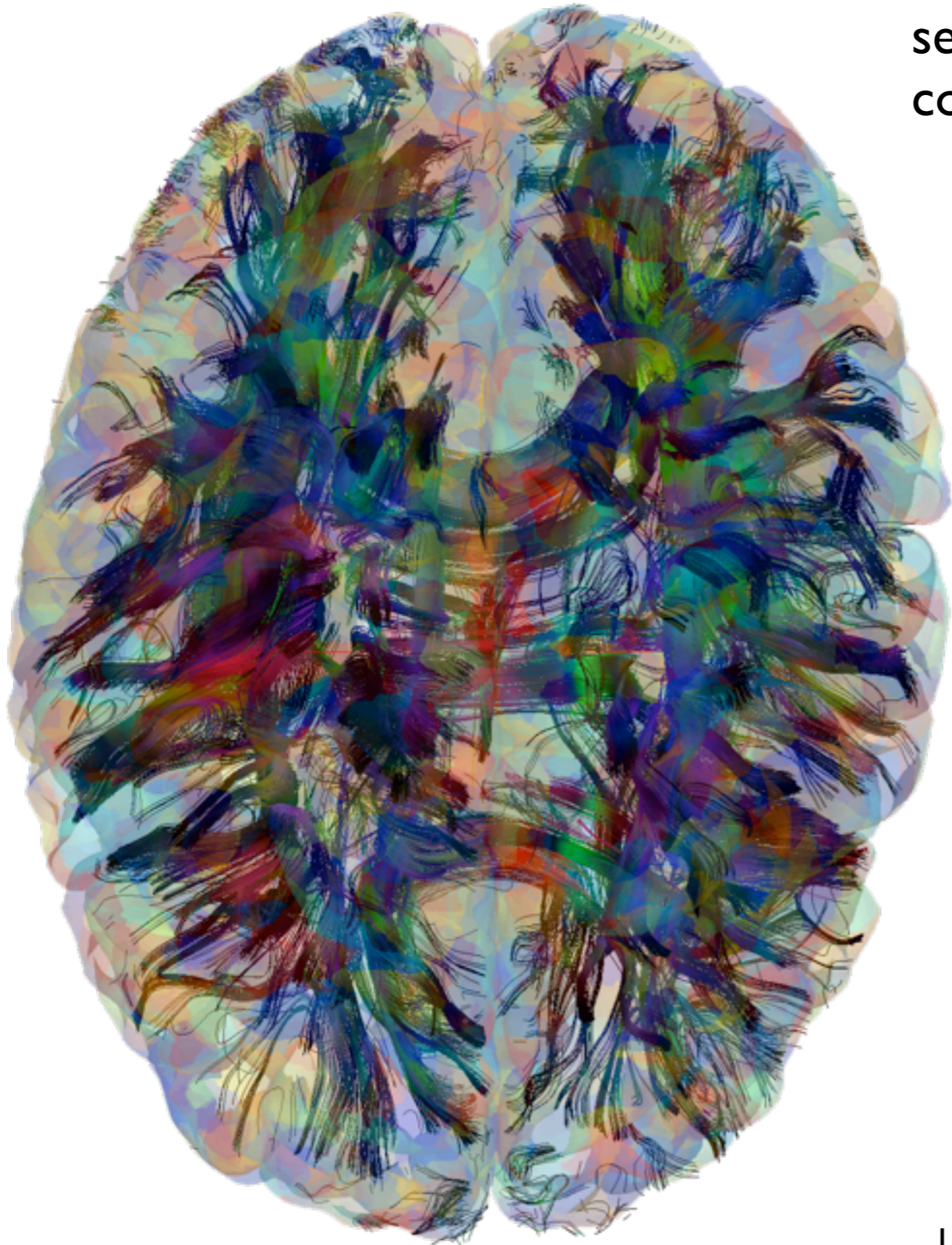
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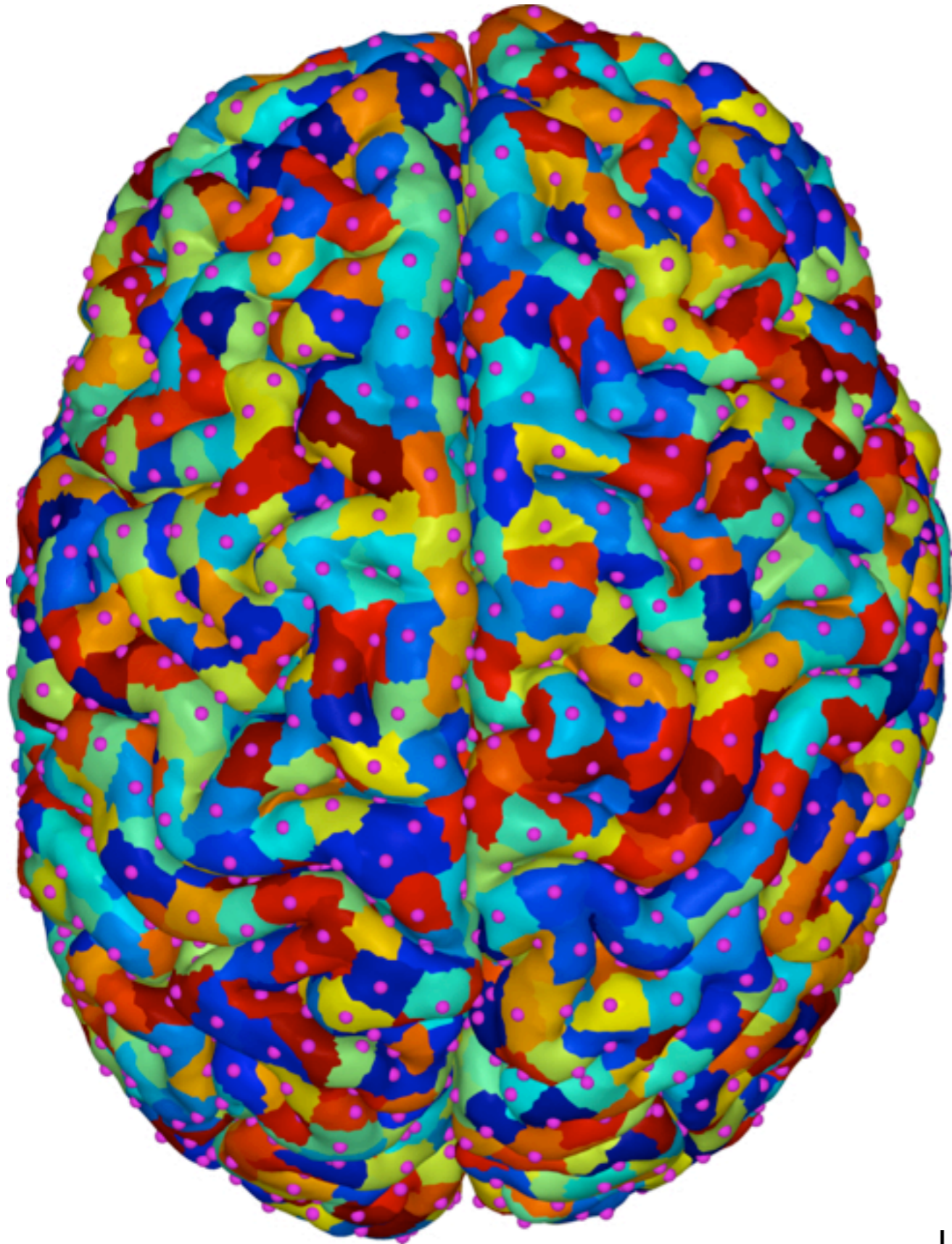
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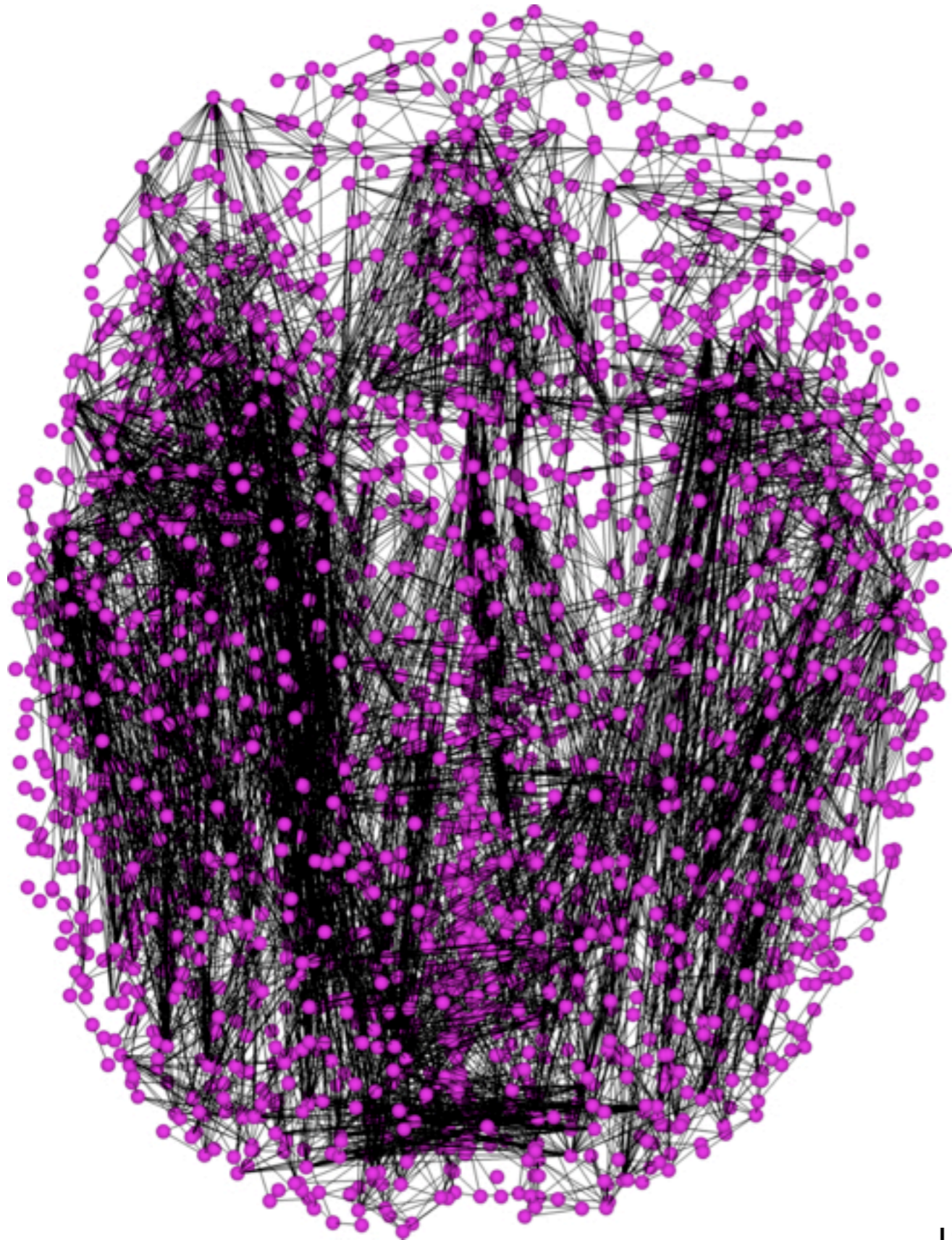


cortex patches, showing patch centers



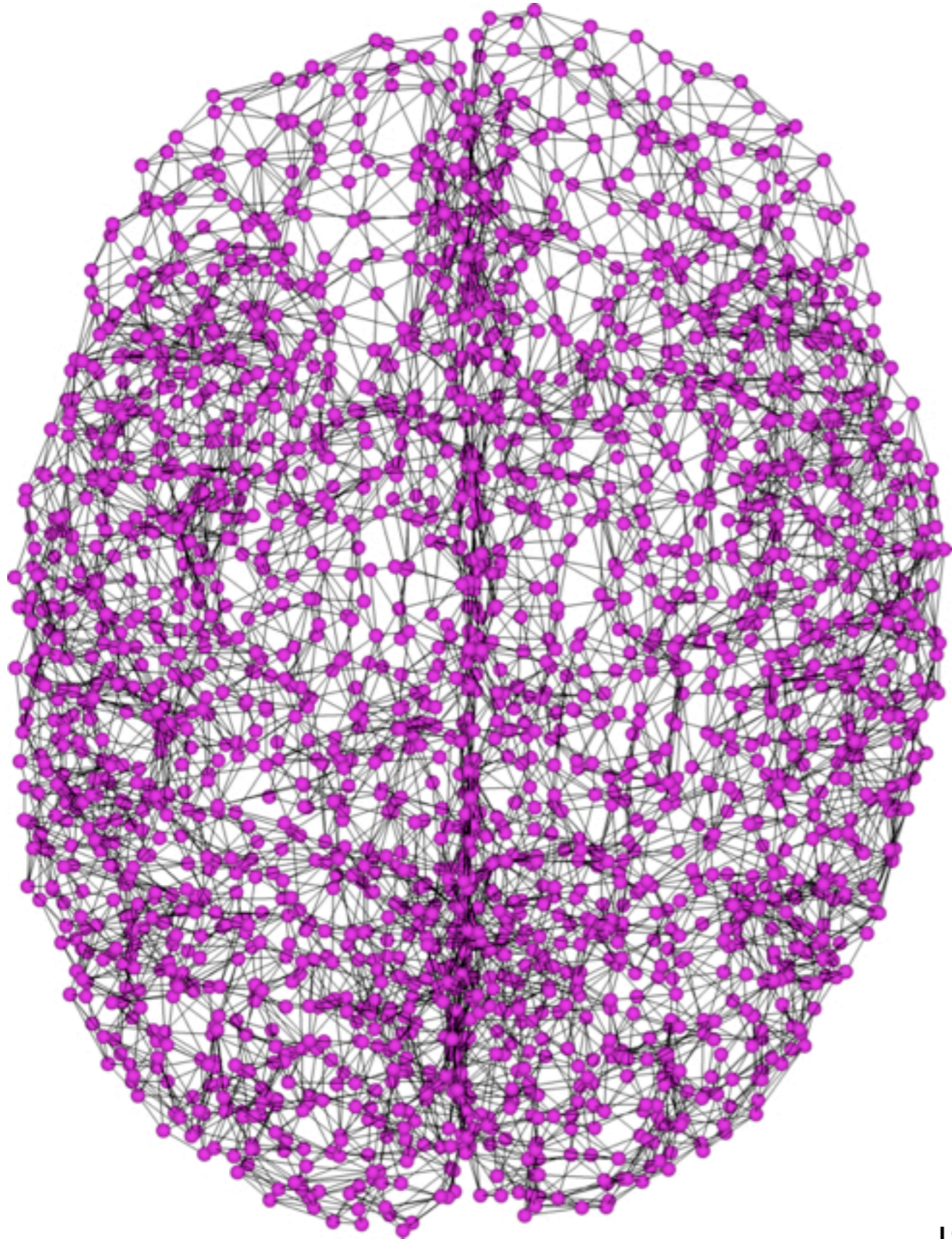


# Global (tract-based) connectome graph





# Local connectome graph



# EEG inverse problem

linear superposition :

$$\Phi = KJ$$

Inverse problem : Given  $\Phi$ , find  $J$

$N_e$  equations,  $N_d$  unknowns  $\Rightarrow$   
infinitely many possibilities for  $J$ !

Find  $J$  minimizing

$$\|\Phi - KJ\|^2 + f(J)$$

data fidelity

prior

$f(J)$  : small for “good”  $J$   
large for “bad”  $J$

how to build prior using connectivity?

# Sparse representation with Cortical Graph Wavelets

Construct SGWT from hybrid connectome  $A$

$$W : \mathbb{R}^{N_d} \rightarrow \mathbb{R}^{K N_d}$$

expand  $J = \sum_i c_i \psi_i = W^T c$

prior :  $\ell_1$  penalty on  $c$

$$c^* = \operatorname{argmin}_c \|\Phi - KW^T c\|_2^2 + \lambda \|c\|_1 \quad (\text{P})$$

$$J^* = W^T c^*$$

(P) is convex, LI-LS program

solve with truncated Newton interior point method

Kim, Koh, Lustig, Boyd,  
Gorinevsky 2007

# Motor Potential study

Phan Luu (EGI)

Validation : investigate source estimates for paradigm where we “know” where the sources should be

Experimental paradigm:

Press button (RT,LT,RP,LP)

EEG recording setup :

256 - channel (257 electrodes) sensor net, 250 Hz

average locked to button press onset (ERP)

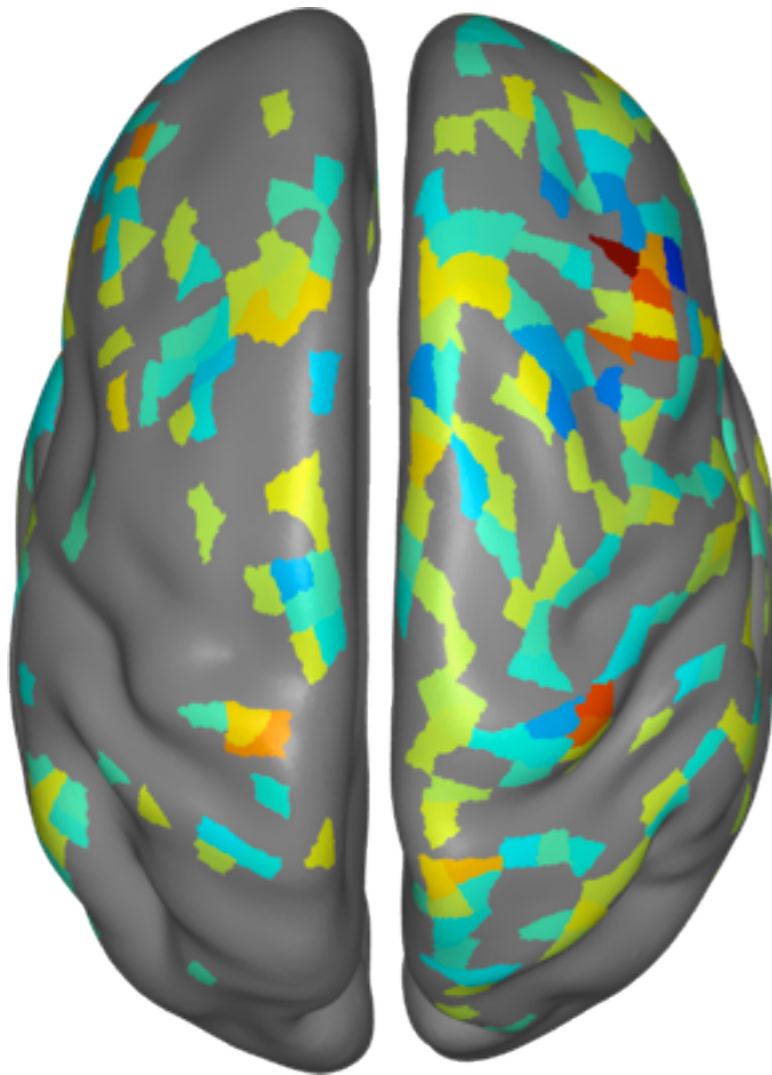
expect activation in contralateral motor cortex



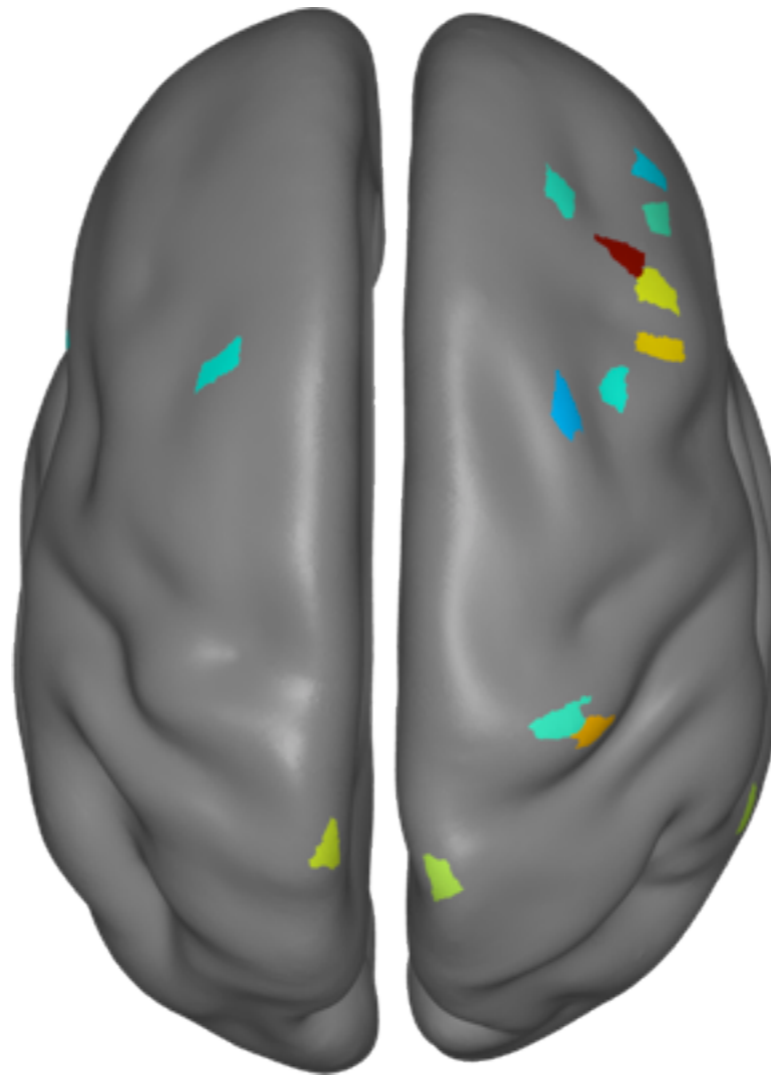
# Preliminary Results

subject  
1470

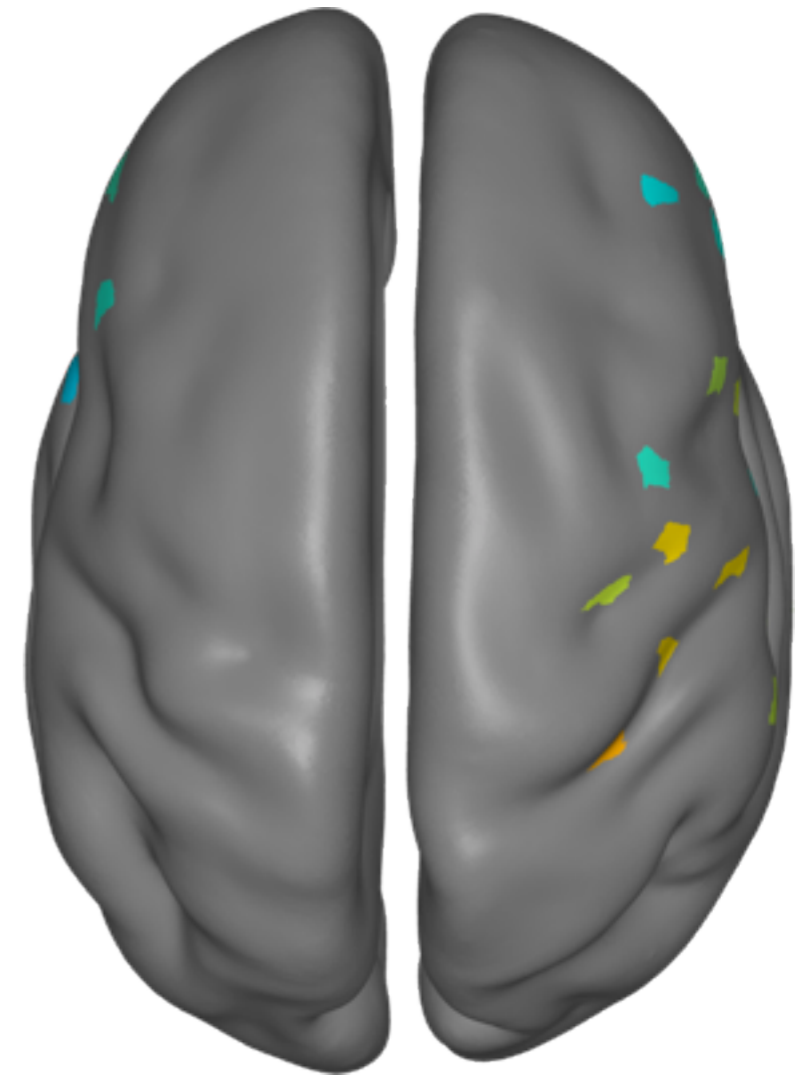
40 ms before left thumb press



minimum norm  
( $l_2$  penalty)



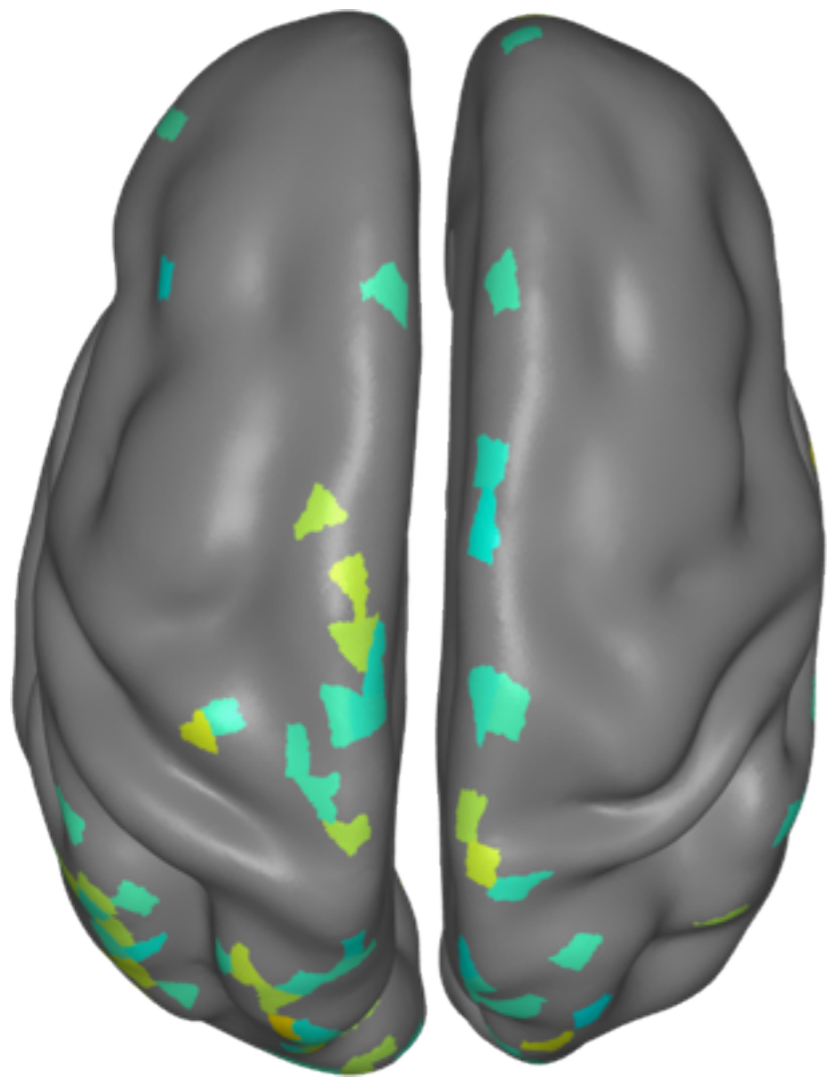
proposed  
(wavelet  $l_1$  penalty)



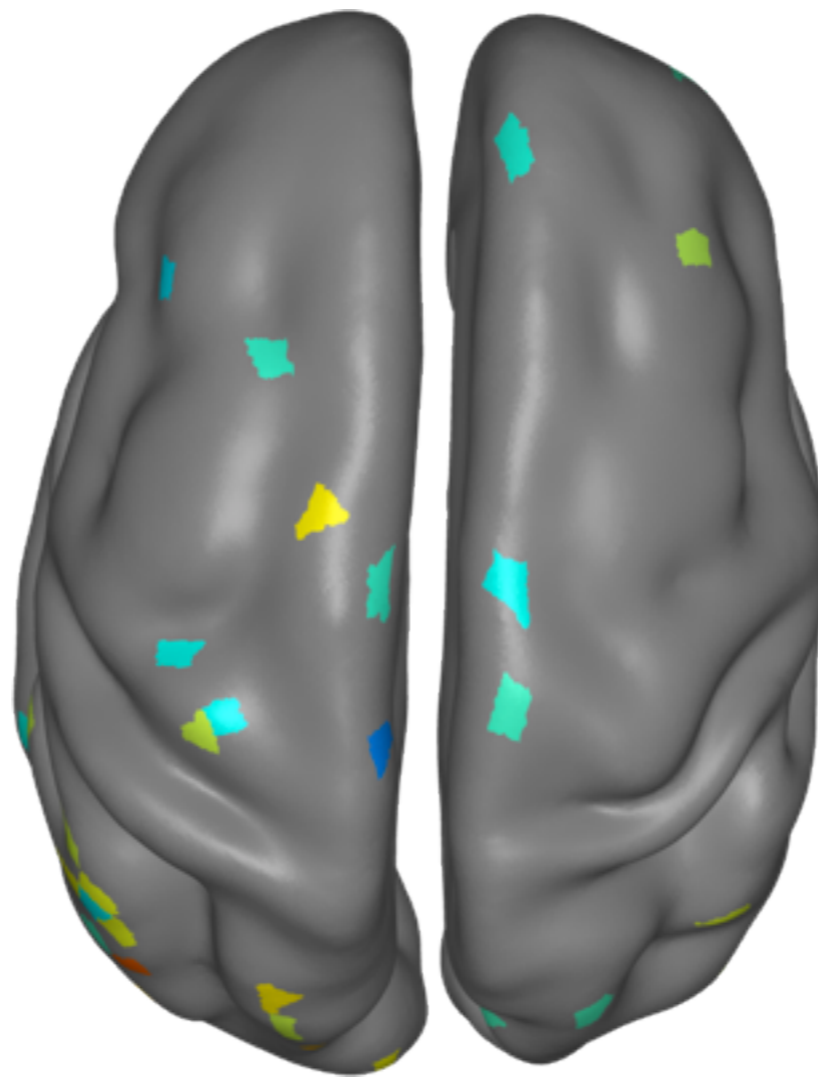
dipole  $l_1$  penalty

subject  
1490

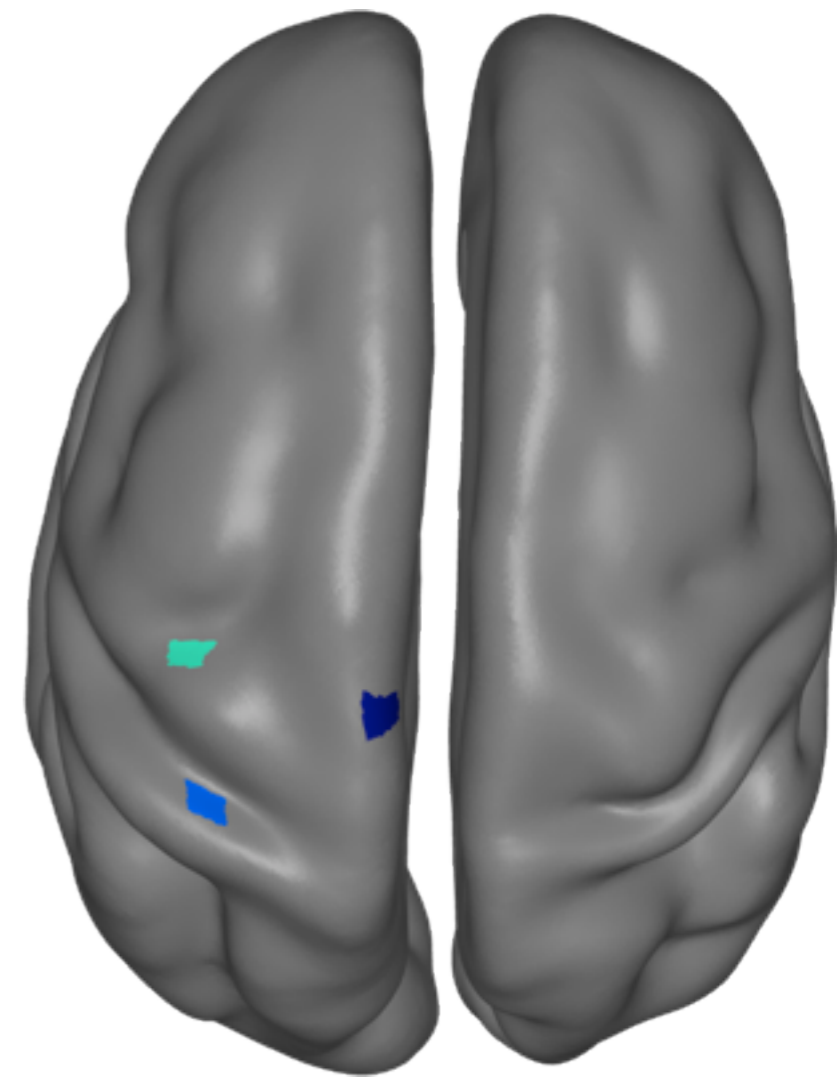
76 ms before right thumb press



minimum norm  
( $l_2$  penalty)



proposed  
(wavelet  $l_1$  penalty)



dipole  $l_1$  penalty



# Future Work

Explore parameters (connectome graph construction, SGWT ...)

Sensible automatic selection of regularization parameters (L-curve)

Spatiotemporal estimation via spatiotemporal graph

More appropriate convex solver (path following for  $\lambda$ )?

Alternative convex program formulations

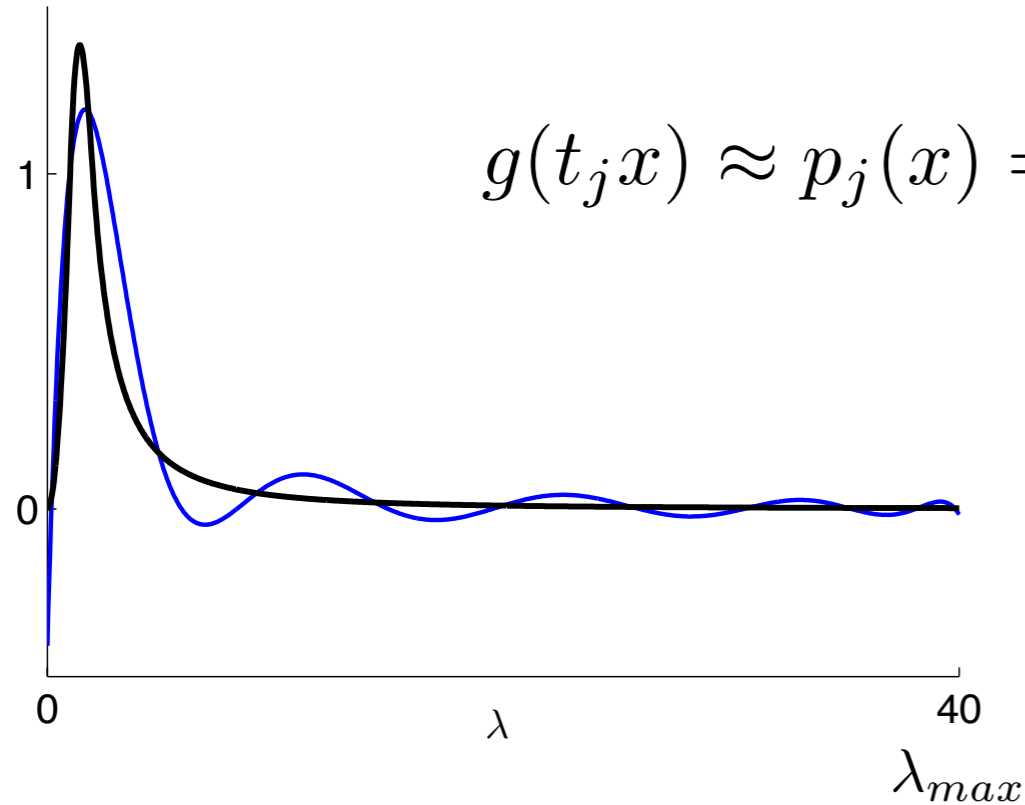
More subjects / different experimental paradigms

# Acknowledgements

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Kai Li	NIC, University of Oregon
Simon Warfield	CRL, Children's Hospital, Harvard
Benoit Scherrer	CRL, Children's Hospital, Harvard

**FIN**

# Chebyshev polynomials for fast SGWT



$$g(t_j x) \approx p_j(x) = \sum_{k=0}^M c_{j,k} T_k(x)$$

Chebyshev approx  
for  $M=10$

$$g(t_j L) f \approx p_j(L) f = \sum_{k=0}^M c_{j,k} (T_k(L) f)$$

$$T_k(x) = 2xT_{k-1}(x) - T_{k-2}(x)$$

$$T_k(L) f = 2L(T_{k-1}(L) f) - T_{k-2}(L) f$$

**computing  $T_k(L) f$  is fast if  $L$  is sparse**

# Some Cortical Graph Wavelets

